




Tuberculosis POCT: An Integrated Photonic Biosensor for Tuberculosis Detection

Ayyasar A. Elamin, D. Martens, A. B. González-Guerrero, M. Stehr, F. Jonas, W. Van Roy, R. Vos, A. Stassen, S. Severi, R. Bockstaele, P. Soetaert, B. Anton, H. Becker, L. M. Lechuga, P. Bienstman, Mahavir Singh







Goal: Point of care test for tuberculosis

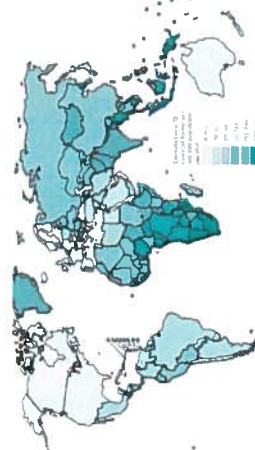



- In 2014, TB killed 1.5 million people (1.1 million HIV-negative and 0.4 million HIV-positive).
- In 2014, 6 million new cases of TB
- TB now ranks alongside HIV as a leading cause of death worldwide.
- Resistance
 - MDR-TB (3.3% of new TB cases and 20% of previously treated cases have MDR-TB)
 - XDR-TB
 - TDR-TB
- Burden of latent infection




Goal: Point of care test for tuberculosis

- Tuberculosis is a global disease
- Current methods for the detection of TB are either time consuming or require expensive instruments (not point of care) and no rapid tests for diagnosis of active TB are available
- World market for Tuberculosis diagnosis: more than 1 billion US\$
- HIV and TB is a deadly combination killing the maximum number of people world-wide due to any infectious diseases




Estimated TB incidence rates, 2014 (WHO, Global tuberculosis report (2015))



Progress beyond state-of-the-art in TB detection

Method	Cost	Information
Culture test (BACTEC MGIT)	- Gold standard	- Costly - Needs instrumentation and a lab - Time consuming
Nucleic acid test (Cepheid GeneXpert)	- Drug resistance information	- Costly (20 euros) - Unsuitable for tropical, TB-endemic countries
Lab-based ELISA Serology	- Cheap (1-2 euros)	- Sensitivity < 60% - Trained personnel - No drug resistance information
Lateral flow tests	- Cheap (2 euros)	- Low sensitivity (30-60%) and specificity (60-90%) - Blood test, urine?? - No drug resistance information



A point of care photonic transducer

Silicon nitride waveguides to use 850 nm light for reduced water absorption

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Novel and highly selective TB biomarker developed

Novel selective antibody cocktail were developed vs Mtb LAM and Ag85 complex

Kinetics characterization of one monoclonal anti-LAM antibody using APS sensors on octet platform

High-quality antibodies with KD around 10^{-9} – 10^{-8}

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Preliminary detection of LAM with photonic biosensor

- Different concentrations of LAM are successfully detected
- Successful detection of 250 pg/ml
- Sufficient Limit of Detection for real urine

[LAM]	$\Delta\lambda$ (nm)
250 pg/ml	0.16
500 pg/ml	0.34
1 ng/ml	0.49
50 ng/ml	0.69
1 μ g/ml	4.89

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Ex-situ functionalization procedure

Incubation with 2 mM of DBCO-PEG₃-NHS in EtOH/H₂O (1:1)

Incubation with 100 μ g/mL of anti85B in PBS

Incubation with ethanalamine

BSA blocking (1 mg/mL)

250 μ L LAM 1 μ g/mL ON

250 μ L LAM 1 μ g/mL OFF

Signal: 1,2

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Development of low-cost point-of-care test for Tuberculosis Diagnosis

Input direction

Input coupler

Output couplers

spectral filters

Sensors

- 750 dies/chip for BIOSiNA
- 150 sensors per wafer
- AWG: 30 channels

7160 μm

6755 μm

Measurement procedure

The camera captures the output from all spectral filter channels

The intensities from different channels are continuously monitored

The peak wavelengths are precisely extracted through an elaborate fitting procedure

The cosine-shape corresponds to the MZI sensor spectrum

Multiplexing

Sensor 1

Sensor 2

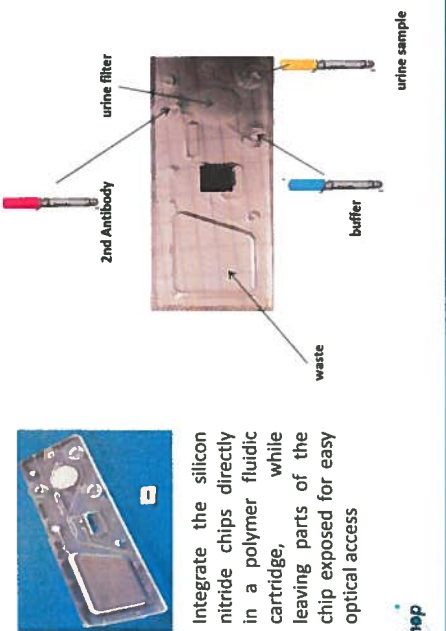
- 2 different sensors measured simultaneously
- 6 sensors present on a single chip
 - Detect multiple antibodies
 - Reference sensor without receptor coating
 - Reduce error

Point of care: The ultimate goal of photonic biosensors

= A device that can be taken to the patient and operated by non-specialists

- Application level**
 - Limited/no sample preparation
- Device level**
 - Easy to use
 - Operational under a range of conditions
- Sensor level**
 - Cheap
 - Disposable
 - Adequate limit of detection

Microfluidic chip as transfer medium

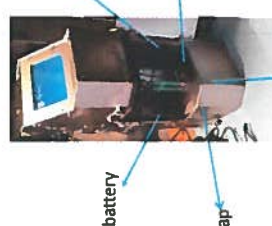


Integrate the silicon nitride chips directly in a polymer fluidic cartridge, while leaving parts of the chip exposed for easy optical access

- 2nd Antibody
- urine filter
- waste
- buffer
- urine sample

ChipShop

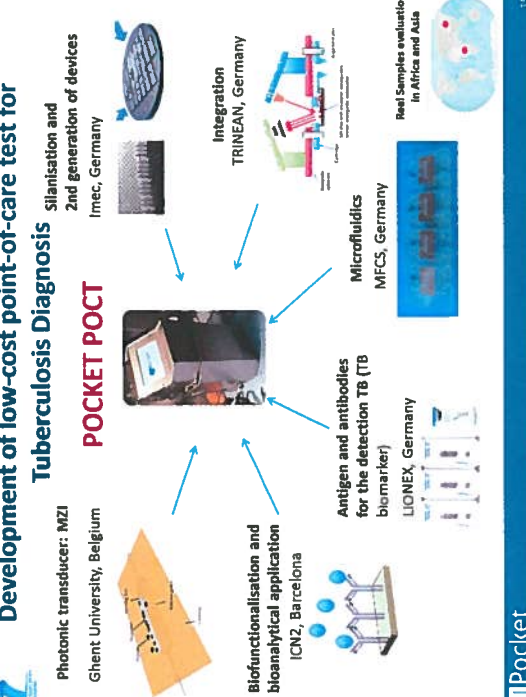
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- Own battery
- No sample preparation
- Easy to use
- Cheap
- Adequate limit of detection

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Development of low-cost point-of-care test for Tuberculosis Diagnosis

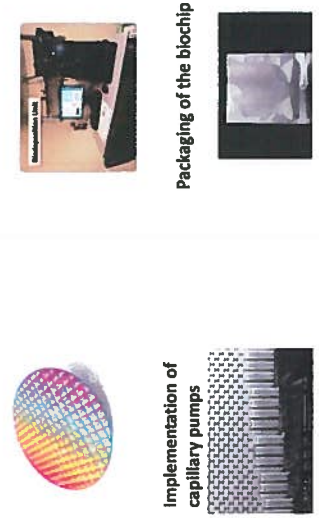


POCKET POCT

- Photonic transducer: NZI Ghent University, Belgium
- Silicisation and 2nd generation of devices Imec, Germany
- Integration TRINEAN, Germany
- Microfluidics MFCS, Germany
- Real Samples evaluation in Africa and Asia
- Antigen and antibodies for the detection TB (TB biomarker) LIONEX, Germany
- Biofunctionalisation and bioanalytical application ICN2, Barcelona

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Towards an industrial process




- Functionalisation at wafer level
- Implementation of capillary pumps
- Spotting of the antibodies
- Packaging of the biochip

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Conclusion and outlook

- Point-of-care photonic sensor with bulk limit of detection of $7 * 10^{-7}$ RIU and potential for multiplexing
- Successful detection of 250 pg/ml LAM, a biomarker for TB found in urine
- Field tests planned in 2017



The image shows a person standing at a podium during a presentation. A laptop on the podium displays the POCAL logo. The person is wearing a dark jacket and glasses. The background is dark, and there are some lights visible.

Thanks



The Pocket logo consists of a blue square with a white outline of a pocket, followed by the word "Pocket" in a white sans-serif font.



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AACC CPOCT INTERNATIONAL SYMPOSIUM

The Benefits and Challenges of Point-of-Care Testing
Across the Clinical Spectrum
September 21-24, 2016, Copenhagen, Denmark
Accepted Abstracts

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SESSION 1: POCT IN THE INTENSIVE CARE SETTING

P1 Allon Reiter: [Diagnosis of Infection Utilizing Accellix
CD64](#)

P2 Paloma Oliver: [Precision and agreement of 266
strip-based glucose meters without the involvement of the
laboratory medicine](#)

P3 Hanneke Buter: [Plasma glutamine levels before
cardiac surgery are related to post-surgery infections; an
observational study.](#)

P4 Nuha Al Humaidan: [Analytical Performance of Point of
Care Blood Gas Analyzers In The Operating Theaters](#)

P5 Zachary O'Brien: [Novel POC Devices for Testing
Procalcitonin \(PCT\) in ER and ICU Settings](#)

P6 James Nichols: [GEM Premier 5000 Clinical Evaluation](#)

P7 Gareth Davies: [Development of an External Quality
Assessment Scheme for POCT Creatinine Whole Blood
Meters](#)

P8 Alex Mewis: [Organization of an external Quality
Control Program for ACT Medtronic](#)

P9 Paloma Oliver: [Differences in blood gas results
between POCT Neonatal Intensive Care Unit and
Emergency laboratory](#)

P31 Jin Xu [Assessment of the performance of Blood Glucose Monitoring Systems for monitoring glycaemia in neonatal patients](#)

SESSION 3: POCT IN THE PRIMARY CARE SETTING

P32 Eunhee Nah [Clinical Value of the Urinary Albumin-to-Creatinine Ratio Measured Using a Strip Test in Prediabetes and diabetes](#)

P33 Kirsi Luttinen-Maunu [Nurse-managed Anticoagulation Clinic in Finland--How Point-of-care testing \(POCT\) affects TTR in Primary Care Setting](#)

P34 Maurice Laville [Creatinine level in capillary blood: a new tool for instant estimation of glomerular filtration rate at home or in ambulatory care settings](#)

P35 Marijana Yucic Lovrencic [Diagnostic performance of a point-of-care glucose analyzer in gestational diabetes](#)

P36 Sanne van Delft [Analytical performance, agreement, and user-friendliness of automated POCT urine test strip analysers, and a comparison between man and machine](#)

P37 Kirsi Luttinen-Maunu [Quality Management of Point-of-care testing \(POCT\) process in nurse-managed anticoagulation clinics](#)



P38 Ayssar Elamin [Tuberculosis POCT: An Integrated Photonic Biosensor for Tuberculosis Detection](#)

P39 Lara Harmans [Implementation of quality assured POC testing in Dutch general practice](#)

P40 Hans van Pelt [Evaluation of three POCT Hematology analyzers for white blood cell analysis](#)

P41 Celine van Lint [Self-monitoring creatinine after kidney transplantation: adherence to measurement protocol and reliability of patient reported data](#)

P42 Anjly Jain [Point of care creatinine testing in screening and monitoring of chronic kidney disease](#)

P43 Javier Segarra [New Emergency departments in primary care: efficiency when enhancing the role of POCT](#)

Tuberculosis POCT: A Potential Application of Integrated Photonic Biosensor for Tuberculosis Detection

A. A. Elamin¹, D. Martens^{2,3}, A. B. González-Guerrero⁴, M. Stehr¹, F. Jonas¹, W. Van Roy⁵, R. Vos⁵, A. Stassen⁵, S. Severi⁵, R. Bockstaele⁶, P. Soetaert⁶, B. Anton⁷, H. Becker⁷, L. M. Lechuga⁴, P. Bienstman^{2,3}, M. Singh¹

¹LIONEX GmbH, Salzdahlumer Str. 196, Building 1A, 38126 Braunschweig, Germany

²Photonics Research Group, Ghent University-IMEC, Technologiepark-Zwijnaarde 15, 9052 Ghent, Belgium

³Center for Nano- and Biophotonics, Ghent University, Technologiepark-Zwijnaarde 15, 9052 Ghent, Belgium

⁴Nanobiosensors and Bioanalytical Applications Group, Catalan Institute of Nanoscience and Nanotechnology (ICN2), CSIC and The Barcelona Institute of Science and Technology, 08193 Barcelona, Spain

⁵IMEC, Kapeldreef 75, 3001 Leuven, Belgium

⁶Trinean NV, Dulle Grietlaan 17/3 9050 Gentbrugge, Belgium

⁷microfluidic ChipShop GmbH, Stockholmer Str. 20, 07747 Jena, Germany

Tuberculosis (TB) is an old but re-emerging global health threat caused by the *Mycobacterium tuberculosis* (Mtb). One third of the world's population is infected with Mtb and new infections occur at a rate of one per second. Despite greatest global health impact of TB, case detection rates are low, posing serious hurdles for TB control. Current methods for the detection of TB are either time consuming or require expensive instruments. Furthermore, these tests have several limitations and perform poorly in populations affected by the HIV epidemic, are thus not suitable for point-of-care diagnosis. Therefore, an accurate, novel, rapid, more sensitive and cost effective diagnostics are urgently needed.

In this respect, the grand goal of the Pocket project is to establish a framework to combine several state-of-the-art concepts for the development of novel and cost-effective point-of-care test for tuberculosis using patients' urine as non-invasive samples. The new tuberculosis POCT consists of a small photonic chip combined with a microfluidic cartridge (disposable part) and a graphical user interface instrument, used for optical readout and data processing (Figure 1). An integrated label-free photonic circuit is used as biosensor, a low-cost mechanism due to its small size and the compatibility with mature CMOS fabrication technology. The sensing circuit is implemented, combining a highly sensitive Mach-Zehnder interferometer with an on-chip spectral filter, hence replacing the conventional tunable laser by a much cheaper broadband light source. Flood illumination on the input grating couplers was used to reduce the cost and increasing POCT compatibility. The successful development of a POCT TB test depends on an Mtb-specific biomarker. Special focus set to the most promising markers; cell wall lipopolysaccharide lipoarabinomannan (LAM) and Ag85 complex. A novel, high-quality and selective antibodies were developed against Mtb LAM and Ag85 complex biomarkers. This unique cocktail promises to significantly enhance the sensitivity and specificity far beyond current TB tests. In a preliminary experiment, sensor chips were functionalised using an Azide-ended silane by vapor phase deposition and antibodies were bio-conjugated by click-chemistry using a PEG-based linker. Initial results indicate the successful detection of 250 pg/ml of LAM antigen, thus demonstrating its potential for use in resource-limited area and for the on-line diagnosis of TB. In the new POCT, the safety of sample process has been successfully implemented using microfluidic chip as transfer medium. The designed chip has very low fabrication costs, allowing cost-effective disposable chips to be fabricated in mass production. This chip is plugged into the measurement tool, which contains the required components for optical readouts, an automated system to circulate the urine into the chip as well as a computer for data processing.

Due to rising health-care costs, all health-care stakeholders are forced to shift their onus from a 'pay for intervention' to a 'pay for performance' model. The highly promising TB POCT need to be evaluated in order to determine a universal threshold, especially in endemic countries as well as performance in the field. Hence, there is a need and justified rationale for performing medium/large evaluation trials which will be our near future step.

Acknowledgement: The Pocket project was funded by the European Commission under grant agreement no FP7 610389.

Attachment: Figure 1: TB POCT Instrument and the disposable chip parts

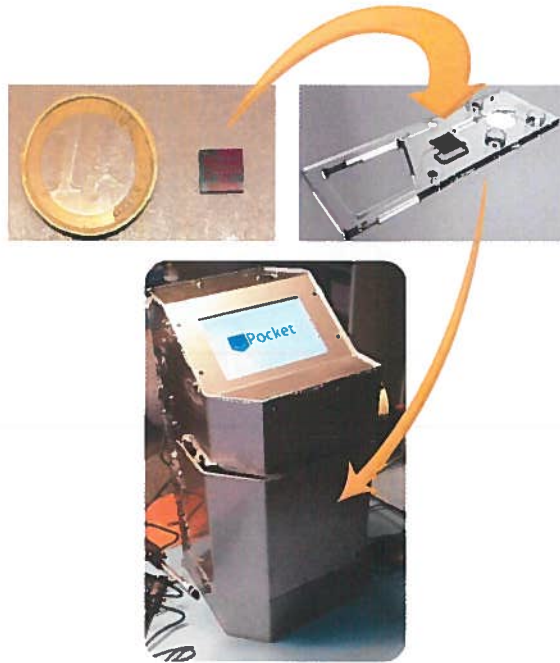


Figure 1: TB POCT Instrument and the disposable chip parts